

SPECIFICATION

TITLE

"CARDIAC STIMULATING DEVICE WITH MORPHOLOGY SENSITIVE DETECTION AND METHOD FOR AUTOMATICALLY CREATING A MORPHOLOGY TEMPLATE"

BACKGROUND OF THE INVENTION

Field of the Invention

The present invention relates to an implantable stimulating device of the type having a morphology sensitive detector for detection of electrical signals originating from the heart. The invention also relates to a method for automatic creation of a template or reference signal for a morphology sensitive detector for cardiac signals.

Description of the Prior Art

The use of morphology sensitive detectors that compare heart signals to a template as a tool to determine the actual heart rhythm is known.

United States Patent No. 5,797,399 discloses a pattern recognition system for use in an implantable cardioverter defibrillator for differentiating between normal and abnormal heart beats. A template standard is established that defines a median or other statistical measure of "central tendency" above which or below which actual sample values would be notable.

United States Patent No. 5,280,792 discloses a method for automatically classifying intracardiac electrograms and a system for performing the method. The method employs neural networks which are trained through the use of supervised training with signals representative for arrhythmia and for normal sinus rhythm.

United States Patent No. 5,240,009 discloses a medical device with morphology discrimination. The intracardiac electrogram is identified by determining, with respect

00003355.11901

to a waveform peak of the intracardiac electrogram, its amplitude, width and polarity. The identification criteria are averaged and stored to provide a standard complex. Subsequent complexes are compared to the stored standard complex. Such comparison includes comparing peaks of subsequent complexes with the peaks of a stored standard complex, aligning subsequent complexes with a stored standard complex, and providing a score associated with the comparisons and alignment.

United States Patent No. 5,645,070 discloses a method of discriminating among cardiac rhythms of supraventricular and ventricular origin by exploiting the differences in their underlying dynamics reflected in the morphology of the waveform. A first cardiac rhythm electrogram of known origin is sensed and a phase space representation or trajectory is generated for use as a template. The template is used for comparison with the current waveform complexes. If the difference is sufficiently different then the rhythm is deemed to be of different origin compared to the template.

United States Patent No. 4,905,708 discloses an apparatus for recognizing cardiac arrhythmias that digitizes analog signals which are obtained when carrying out sensing at the heart or on the body and carries out a first differentiation of the digitalized signals. The concept is to compare the first differential of the digitized electrogram of each heartbeat with what is established to be the first differential of the digitized electrogram for normal rhythm.

In a master thesis by Joakim Lingman at the Royal Institute of Technology, Department for Signals, Sensors, & Systems, an improved heartbeat detector is disclosed. A matched filter for heart beat detection is disclosed. In order to obtain a template for the matched filter, a prerecorded digitized IEGM of a certain length is divided into three parts. Around the sample value with the highest negative derivative

Figure 3 shows a schematic flowchart of the most basic algorithm of the invention.

Figure 4 shows a schematic flowchart of an implementation specifically designed to adapt to signals with a high baseline drift.

Figure 5 shows a schematic flowchart of an implementation similar to the implementation outlined in figure 3 but with a filter added to improve noise rejection.

Figure 6 shows a schematic flowchart of an implementation as outlined in Figure 4 but with a filter added to improve noise rejection.

Figure 7 shows a schematic flowchart of how the algorithm described in figure 5 can be improved by adding a step of shifting selected deflections for optimum alignment with the current template used by the filter before updating the template with the selected deflection.

Figure 8 shows a schematic flowchart of how the algorithm described in figure 6 can be improved by adding a step of shifting selected deflections for optimum alignment with the current template used by the filter before updating the template with the selected deflection.

Figure 9 shows a schematic flowchart of a shifting algorithm used to optimize the alignment between signal and template. This will potentially improve the quality of the resulting template.

Figure 10 shows a schematic flowchart of how selected deflections may be divided into different classes, using the generalized Lloyd algorithm, for a later determination of which class or classes that is most representative for physiologic heart signals.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

Figure 1 shows a typical pacemaker system as implanted. The pulse generator 14 is connected to the heart via a lead body 13 and an electrode 11 connected to the distal portion of the lead body 13. Signals from a patient's heart 12 are picked up by the electrode 11 and transferred to the pulse generator 14 by the lead body 13. Stimulation pulses from the pulse generator 14 are transferred to the heart 12 via lead body 13 and electrode 11. The pacemaker also includes a heart signal detector 25. The present invention forms a part of this heart signal detector.

Figure 2 shows a signal processing hardware block diagram that can be used to implement the invention, including the lead body 13, an A/D-converter 21, a memory 22, a CPU 23 and a template storage 24 that is a part of the heart signal detector 25. Basically the processing involves two steps. The first step is when the heart signal obtained from the lead body 13 is continuously A/D converted in the A/D converter 21 and stored in a memory 22. This step corresponds to an operation that can be described as recording of an IEGM segment. In the second step different algorithms implemented as software in the CPU are applied on the signal stored in the memory 22 to create the signal template stored in the signal template storage 24 to be used by the heart signal detector 25.

Figure 3 shows a schematic flowchart of the first part of the algorithm to determine a template for a filter matched to a certain morphology. A matched filter is a filter that has its maximum gain for a signal identical to the template. The purpose of this diagram is to define a method to select deflections that may be QRS-complexes in an amplitude descending order. In block 31 a segment of an IEGM signal is recorded, the length of which may be in the range from a few seconds up to several

minutes. Following the recording the recorded signal may be filtered in a filter suitable for intracardiac signals in order to remove noise and to enhance portions of the signal. The filtering can be made by digital filtering by the CPU 23 (Fig. 2) on the recorded signal in the memory 22 (Fig. 2) for flexibility reasons since that allows the filter parameters to be modified after recording but it would also be feasible to make the filtering through hardware filters simultaneously with the recording. In block 32 the largest deflection is identified and selected. In block 33 all deflections in the signal with an amplitude exceeding a predetermined percentage in the range of 40-75 % of the maximum amplitude in the recorded signal are to be found and stored for subsequent analysis. When performing this step the maximum amplitude must be checked to be within reasonable limits. In block 34 deflections are selected in descending order. In order to reject signals which are not of physiologic origin, deflections which are closer than a predetermined time interval, e.g. approximately 350 ms to a previously selected deflection, are excluded from selection. The time interval may be in the range 200-500 ms. The selection process ends either when no more deflections will be taken into account since they fall within the time interval mentioned above, or when the amplitude of the remaining deflections are less than a predetermined percentage of the maximum signal amplitude recorded. In block 35 all selected deflections are stored for further analysis.

The final result from the process outlined in Figure 3 is a number of possible heart signal deflections that may be used for template generation.

Figure 4 is an enhanced schematic flowchart that would improve the functionality in the presence of large amplitude variations in the IEGM-signal recorded from the

electrode. This is achieved by always searching for the highest deflection in the longest interval found between two previous selections.

In block 41 an IEGM segment is recorded. This is accomplished through continuous AD-conversion of the incoming signal. The AD-converted signal values are written into the memory 22 (Fig.2). The second optional step may be to filter the recorded signal in a filter suitable for signals of cardiac origin. The filtering is typically digital filtering performed on collected data. Digital filtering means that the CPU 23 performs mathematical operations that are equivalent to filtering on the stored IEGM segment. In block 42 the largest signal deflection is selected. In block 43 the longest interval between two selected deflections or between an endpoint in the recording and a selected deflection is identified. In this interval the largest deflection is selected that is not closer to a previously selected deflection than a predetermined interval in the range of 200-500 ms.

In block 44 and in block 45 the process to identify the longest interval and to select the largest deflection in the longest interval continues until one of the two following conditions is fulfilled: a) the average interval between selected deflections is shorter than a predetermined value in the range of 1000-2000 ms and the maximum interval is shorter than a predetermined value in the range of 1500-3000 ms or b) if the average interval is shorter than an interval in the range 400-800 ms. In block 46 all selected events are stored for further analysis. The final result from the process outlined in Figure 4 is a number of possible heart signal deflections that may be used for template generation.

Figure 5 represents an enhancement of the algorithm described in Figure 2. Basically the enhancement is that a filter is introduced in the deflection selection

Figure 5 is a number of possible heart signal deflections that may be used for template generation.

Figure 6 represents an enhancement of the algorithm described in Figure 4. Basically the enhancement is that a filter is introduced in the deflection search. In block 61 an IEGM segment is recorded that may have a duration between a few seconds up to several minutes. In block 62 the largest deflection is identified and selected. In block 63 the largest of the remaining deflections that is separated from the first selected deflection with at least a predetermined value in the range of 200-500 ms is identified and selected. In block 64 a provisional template for creation of filter parameters is created based on selected deflections through averaging. In block 65 the longest interval between two selected deflections is identified. Further in block 65 the largest deflection after processing the signal in the filter is selected. Finally the provisional template is updated based on selected deflections in block 65. In block 66 a test is performed to determine if the number of selected deflections is less than a predetermined value in the range of 4-15. Block 65 is repeated as long as the number of selected deflections is less than the predetermined number in the range of 4-15. After having reached a predetermined number in the range of 4-15 selected deflections the algorithm continues in block 67 as described above with the modification that a predetermined percentage in the range of 60-80% of the deflections selected that deviates least from the average of all selected deflections are used when the provisional template used for determination of the filter parameters is created. In block 68 the following test is performed: the process to identify the longest interval and to select the largest deflection in the longest interval continues until a) the average interval between selected deflections is shorter than a predetermined value in the range of

1000-2000 ms and the max interval is shorter than a predetermined value in the range of 1500 – 3000 ms or b) if the average interval is shorter than an interval in the range 400 - 800 ms. The final result from the process outlined in Figure 6 is a number of possible heart signal deflections that may be used for template generation.

Figure 7 illustrates a technique to further enhance the performance of the algorithm described in Fig 4 particularly under noisy conditions. If noise is present the peak amplitude may occur at a different point in time compared to when no noise is present. As a result the resulting template will become distorted. One possibility to minimize the effect of superimposed noise would be to shift a selected complex to the left or right and after each shift operation calculate the Euclidean norm between the selected complex and the current provisional template and select the shifted complex that gave the minimum Euclidean norm. The amount of shifting expressed in time should be limited to a predetermined interval in the range of 0 -15 ms. When the provisional template is updated by adding the selected complex this will be optimally aligned to the current provisional template which will improve the quality of the updated template. Thus as soon as a deflection is selected it will be shifted for optimum alignment with the current provisional template before the selected deflection is used for provisional template updating. In block 71 an IEGM segment is recorded and stored in the memory. In block 72 the largest deflection is identified and selected. In block 73 the largest of the remaining deflections is identified and this deflection is selected if it is not closer than a predetermined interval in the range of 200-500 ms to a previously selected deflection. In block 74 a provisional template for the filter is created based on the selected deflections. In block 75 the largest of the not selected deflections after processing the signal in the matched filter is identified. This deflection

deflection is selected if it is not closer than a predetermined interval in the range of 200-500 ms to a previously selected deflection. In block 84 a provisional template for determination of filter parameters is created based on the selected deflections. In block 85 the longest interval between two selected deflections is identified. The largest deflection after processing the signal in the filter is selected if it is separated from a previously selected deflection with at least a predetermined value in the range of 200-500 ms. Further in block 85 the Euclidean distance is calculated between the current template and the selected deflection. The selected deflection is shifted back and forth in an iterative procedure until the lowest value of the Euclidean distance is found. The final activity in block 85 is to update the provisional template as an average of all selected deflections for determination of filter parameters. In block 86 a test is performed to determine if the next block to be processed shall be block 85 repeated or if the next block to be processed shall be block 87, if the number of selected deflections is less than a predetermined number in the range of 4-15 the next block to be processed shall be block 85 otherwise the next block to be processed shall be 87. In block 87 the part of the stored signal with the longest interval between two selected deflections is identified. The largest deflection after processing the signal in the matched filter is selected if it is separated from a previously selected deflection with at least a predetermined value in the range of 200-500 ms. Further in block 87 the Euclidean distance is calculated between the current provisional template and the selected deflection. The selected deflection is shifted back and forth in an iterative procedure until the lowest value of the Euclidean distance is found. Next activity in block 87 is to update the provisional template for determination of the filter parameters. The template is created from the average of a predetermined percentage in the range

of 60-80 % of the selected deflections that are most similar to the current template. In block 88 the following test is performed: the process to identify the longest interval and to select the largest deflection in the longest interval continues until a) the average interval between selected deflections is shorter than a predetermined value in the range of 1000-2000 ms and the max interval is shorter than a predetermined value in the range of 1500 – 3000 ms or b) if the average interval is shorter than an interval in the range 400 - 800 ms. When the criteria in the test are fulfilled the process to find deflections is finalized. The final result from the process outlined in Figure 8 is a number of possible heart signal deflections that may be used for template generation.

Figure 9 illustrates another way to improve the quality of the template. In block 91 a template created as an average of all selected deflections. In block 92 each deflection is shifted to find the minimum of the Euclidean norm between the selected deflection and the current template. The amount of shift allowed in block 92 is limited to ± 15 ms. In block 93 a new template is created as the average of all selected deflections after shifting. The procedure in block 92 and 93 may be repeated to further improve the quality of the template. This method is applicable to improve the quality of the template regardless of how the deflections has been selected.

In Figure 10 a technique is provided to divide all selected deflections into classes. The idea is then to select the most QRS-like class as basis for the template. After identification and storing of deflections that may originate from these potential QRS are divided into a predetermined number of classes. The number of classes should be selected in range 1-10 and may depend on the current noise situation. In a preferred embodiment the Generalized Lloyd Algorithm (GLA) has been used for classification of the signals. Figure 10 illustrates the application of the GLA algorithm

to divide selected deflections into classes. In block 101 an initial set of class centers is selected e.g. at random. In block 102 all selected deflections are assigned to the class they are closest to. In block 103 new class centers are calculated based on the average of the deflections in respective class. In block 104 each of the selected deflections is assigned to the class it is closest to. In block 105 a test is performed to determine if the process of assigning the selected deflections to different classes can be finalized. If no deflections changed classes in the last processing of block 104 the procedure of dividing the selected deflections into classes shall be terminated otherwise the procedure of dividing the selected deflections into classes will continue with block 103.

Following the classification of the deflections the most representative class for the QRS shall be selected. Several different criteria for selection of the most representative class may be defined. High amplitude and morphological similarity has shown to be useful criteria for selection of the most representative class. In one preferred embodiment the class for which the mean amplitude divided by the normalized dissimilarity resulted in the largest number was selected as the most representative class for the creation of the template for the morphology sensitive detector. The normalized dissimilarity in a class is defined as the mean of the squared distance between the average and the individual deflections in the class. Normalization means dividing the individual deflections by the square root of the sum of the squares of the deflections in question. Other possible criteria would be to study the repetition rate for the deflections belonging to a particular class in which case deflections with a repetition rate reasonable for a beating heart would be an indicator that the class might be representative. Studying the mean maximum derivative in the class for each

deflection could also be possible, a higher mean maximum derivative indicating a higher probability that the complex is a true QRS.

Although modifications and changes may be suggested by those skilled in the art, it is the intention of the inventor to embody within the patent warranted hereon all changes and modifications as reasonably and properly come within the scope of his contribution to the art.

0093156-11101